



An innovative method of density of biomedical metaphors with shrill steadfastness by hop

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Abstract

Novel hierarchical oriented prediction approach to resolution scalable lossless and near-lossless (NLS) compression. It joins the flexibility of DPCM plans with new various leveled arranged indicators to supply goals versatility with preferred pressure exhibitions over the standard progressive interjection indicator or the wavelet change. Medical images of CT scan and MRI images are preprocessed using speckle reducing anisotropic diffusion (SRAD). The proposed various leveled arranged forecast (HOP) isn't generally proficient on smooth pictures, so we introduce new predictors of HOP-LSE, HOP-LSE+, which are dynamically optimized employing a least-square criterion. The HOP algorithm is well suited for NLS compression and provides the high-resolution images. Here calculate the compression ratio using bits per pixel and peak signal to noise ratio. Finally, when compared those compression methods, we got the better compression ratio in HOP-LSE+.

Keywords: NLS compression, DPCM, SRAD, HOP, JPEG and wavelet transform

1. Introduction

An uncompressed multimedia (graphics, audio and video) data requires considerable storage capacity and transmission bandwidth. In spite of quick advancement in mass-stockpiling thickness, processor velocities, and information correspondence framework execution, interest for information stockpiling limit and information transmission data transfer capacity keeps on exceeding the abilities of possible advances. The ongoing development of information serious interactive media-based web applications haven't just supported the requirement for increasingly proficient approaches to encode signals and pictures however have made pressure of such signals vital to capacity and correspondence innovation. For still pressure, the Joint Photographic Experts Group (JPEG) standard has been built up by ISO (International Standards Organization) and IEC (International Electro-Technical Commission). The performance of those coders generally degrades at low bit-rates mainly due to the underlying block-based Discrete Cosine Transform (DCT) Scheme. More recently, the wavelet transform has emerged as a leading edge-based technology, within the field of image compression. Wavelet coding provides substantial improvements in picture quality at higher compression ratios.

1.1 Need for Compression

In recent years, digital images are becoming more and more important. Digital cameras are now rather cheap and technically mature. As a consequence, digital images are replacing conventional analog images in almost every field. Examples range from holiday pictures to medical images, like x-ray tomography, CT, MRI, and PET. So, there is a natural need to store images on a computer and also to transmit them over the internet, to share them with other persons. Advance medical imaging requires storage of huge quantities of digitized clinical data. Because of the data transfer capacity and capacity confinements, clinical pictures must be packed before transmission and capacity. The main reason of compression algorithms need —natural

images is the presence of image boundaries (edges) and flat regions (plateaus) there. The edges kind of subdivide the image into regions and hence are the semantically important parts. The idea is then to code only these for human observer important parts and neglect the rest, which reduces the amount of data needed.

1.2 Fundamentals of Image Compression Technique

A digital image, or bitmap, consists of a grid of dots, or pixels, with each pixel defined by a numeric value that provides its color. The term data compression refers to the method of reducing the quantity of knowledge required to represent a given quantity of data. Now, a specific piece of data may contain some portion which isn't important and may be comfortably removed. All such data is referred as Redundant Data. Data redundancy may be a central issue in digital compression. Image compression research aims at reducing the quantity of bits needed to represent an image by removing the spatial and spectral redundancies the utmost amount as possible. A typical attribute of most pictures is that the neighboring pixels are associated and subsequently contain excess data. The foremost task then is to seek out less correlated representation of the image. In general, three types of redundancy can be identified:

- Coding Redundancy.
- Inter Pixel Redundancy.
- Psych visual Redundancy

1.2.1 Coding Redundancy

If the grey levels of a picture are coded during a way that uses more code symbols than absolutely necessary to represent each gray level, the resulting image is claimed to contain coding redundancy. It is nearly always present when an image's gray levels are represented with a straight or natural code. Let us assume that a random variable r K lying in the interval $[0, 1]$ represents the gray levels of an image and that each r K occurs with probability $\text{Pr}(r K)$. $\text{Pr}(r K) = N_k / n$ Where $k = 0, 1, 2, \dots, L-1$ (1.1) $L = \text{No. of gray levels.}$ $N_k = \text{No. of times that gray appears in that image.}$

Where, N = Total no. of pixels in the image If no. of bits went to represent each value of r K is $l(r K)$, the typical no. of bits required to represent each pixel is $L_{avg} = l(r K) Pr(r K)$. (1.2). That is average length of code words assigned to the various gray levels is found by summing the product of the no. of bits went to represent each gray level and therefore the probability that the grey level occurs. Thus, the total no. of bits required to code an $M \times N$ image is $M \times N \times L_{avg}$.

1.2.2 Inter Pixel Redundancy

The Information of any given pixel can be reasonably predicted from the value of its neighboring pixel. The information carried by a private pixel is comparatively small. In order to scale back the inter pixel redundancies in a picture, the 2- D pixel array normally used for viewing and interpretation must be transformed into a more efficient but usually non visual 'format.

1.2.3 Psycho visual Redundancy

Certain data just has less relative significance than other data in typical visual preparing. This information is claimed to be Psycho visually redundant, it are often eliminated without significantly impairing the standard of image perception.

1.3 Image Compression Techniques

There are basically two methods of Image Compression, Namely, one is Lossless Coding Techniques and another is Lossy Coding Techniques.

1.3.1 Lossless Coding Techniques

In Lossless Compression schemes, the reconstructed image, after compression, is numerically just like the first image. However Lossless Compression are able to do a modest amount of Compression. Lossless coding guaranties that the decompressed image is completely just like the image before compression. This is a crucial requirement for a few application domains, e.g. Medical Imaging, where not only top quality is within the demand, but unaltered archiving may be a legal requirement. Lossless techniques can also be used for the compression of other data types e.g. text documents and program executable. Lossless compression algorithms are often wont to squeeze down images then restore them again for viewing completely unchanged.

1.3.2 Lossy Coding Techniques

Lossy strategies cause picture quality debasement in every Compression/De-pressure step. Careful consideration of the human beholding ensures that the degradation is usually unrecognizable, though this relies on the chosen compression ratio. An image reconstructed Lossy compression contains degradation relative to the original. Often this is often because the compression schemes are capable of achieving much higher compression. Under typical survey conditions, no noticeable misfortune is seen (outwardly Lossless).

1.4 Prevailing Method

This Lossy compression is an encrypted image with flexible compression ratio. Pseudorandom changes are utilized to encode a clever picture, and in this manner the scrambled information are productively compacted by disposing of the too much unpleasant and fine data of coefficients created

from symmetrical change. In the wake of accepting the packed information, with the help of spatial connection in normal picture, a receiver can reconstruct the principal content of the primary image by iteratively updating the values of coefficients. This way, the upper the compression ratio and therefore the smoother the first image, the higher the standard of the reconstructed image. But this approach does not perform well for medical images.

Several compression methods for 3-D medical images have been proposed in the literature, some of which provide resolution and quality scalability up to lossless reconstruction. These methods are based on the discrete wavelet transform (DWT), whose inherent properties produce a bit-stream that is resolution-scalable. Quality scalability is then achieved by employing bit-plane based entropy coding algorithms that exploit the dependencies between the location and value of the wavelet coefficients, such as the embedded zero tree wavelet coding (EZW), the set partitioning in hierarchical trees (SPIHT), and the embedded block coding with optimized truncation (EBCOT) algorithms. These compression methods, however, do not provide VOI decoding capabilities, i.e., the ability to reconstruct a VOI at higher quality than the rest of the 3-D image. Recently, variety of medical compression methods that support VOI coding are proposed.

In previous systems, the authors presented a compression method based on JPEG2000 that supports prioritized VOI coding based on the anatomical tissues depicted in a 3-D medical image. The method employs a one-dimensional DWT (1D-DWT) along the slice direction with JPEG2000 encoding of the resulting transform slices. A priority is assigned to every group of coefficients describing an equivalent spatial region at an equivalent decomposition level consistent with its intensity within the spatial domain. The technique likewise takes into consideration the meaning of the overall significance of each sub-band in the coding procedure.

The authors introduced a 3-D medical image compression technique that supports VOI coding based on 3-D sub-band block hierarchical partitioning (3D-SBHP), a highly scalable wavelet transform based entropy coding algorithm. A number of parameters that affect the effectiveness of VOI coding are studied, including the dimensions of the VOI, the amount of decomposition levels, and therefore the target bit-rate. The authors also discussed an approach to optimize VOI decoding by assigning a decoding priority to the different wavelet coefficient bit- planes.

The authors summarized the features of various methods for VOI coding, including the maximum shift (MAXSHIFT) and general scaling-based (GSB) methods supported by the JPEG2000 standard. These particular methods proportion the coefficients related to a VOI above the background coefficients, by a scaling value. The MAXSHIFT method employs a maximum scaling value so that VOI coefficients are completely decoded before any background coefficients. The GSB method, on the other hand, employs a lower scaling value so that VOI and background coefficients are decoded simultaneously. The creators introduced a VOI coding technique for volumetric pictures dependent on the GSB strategy and the shape-versatile wavelet change. The method extends the capabilities of the GSB method to 3-D images with arbitrarily- shaped VOIs and allows for coding partial background information in conjunction with the VOI.

2. Related Work

2.1 Interleaved Hierarchical Interpolation (IHINT)

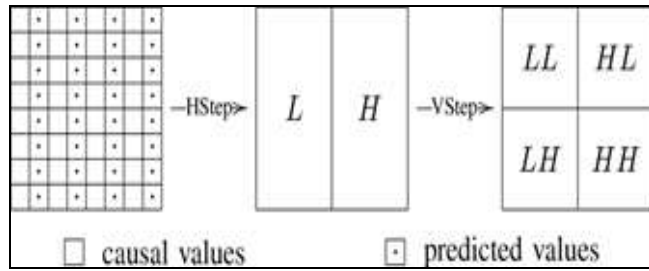


Fig 1: IHINT Algorithm Model

To hierarchically decompose a picture, prediction levels of IHINT are often summarized within the two prediction steps. Let be the set of horizontally even indexed pixel values, and let be the set of horizontally odd indexed pixel values; the first step (H Step) consists of predicting the pixels of using an interpolative finite impulse response filter on. This contains the residual values of the prediction. The second step (V Step) is the mathematical transposition of H Step applied independently on L to obtain two sets. LL and LH, and on H to obtain HL and HH onto obtain.

The set LL then contains a subsampled lower resolution image that can be recursively decomposed. The pixel values/residual of every set are often reorganized to get a dyadic representation. For comparisons to be held within the following, the IHINT prediction of an odd indexed value is that the average of its two (even indexed) neighboring values.

2.2 Hierarchical Oriented Prediction

Like IHINT a forecast degree of the HOP plot is acted in two stages The first one (H Step) comprises of foreseeing on a level plane odd filed pixels esteems with the guide of definitely known pixels: the proposed approach utilizes the even listed ones as well as exploit any recently anticipated ones (which are presently causal qualities). Thus, we will obtain a horizontally subsampled image and therefore the residual of the odd predicted pixels. The second step (V Step) is the mathematical transposition of H Step and acts on the lower resolution image.

Similar to IHINT, HOP can be computed in the same memory space as the image, but it requires that the current row (or column) and the previous ones that are necessary for the prediction are buffered (it represents here a complete of three rows).

3. Problem Statement

3.1 Image Processing

The initial process is preprocessing the input image, for better performance. The input image has different contents and different format. Sometimes the same image is given twice with some small change in that image, but the comparison of these two images using pixel by pixel may not give the positive result. So the proposed methods with few enhancement techniques that enhance the image and then compare the image using only the modified images not the original one.

3.2 Image preprocessing Techniques

The data set images are taken CT scan or MRI images. The dot diminishing anisotropic dispersion channel was as of

late proposed to adjust the anisotropic dissemination channel to the attributes of the dot commotion present inside the ultrasound pictures and to encourage programmed preparing of pictures. The acquisition of ultrasound images introduces a selected noise referred to as speckle.

The statistics of the speckle noise, modeled by, can be categorized into different classes according to the number of scatters per resolution cell also called the scatter number density (SND), to their spatial distribution and to the characteristics of the imaging system. In the case of many fine randomly distributed scatters per resolution cell (> 10), the speckle can be modeled by a Rayleigh distribution Compared to Perona and Malik’s anisotropic diffusion, the SRAD has the advantage of avoiding the edge on the norm of the gradient needed for the diffusion function.

This threshold is replaced by an estimation of the standard deviation of the noise at each iteration which gives to SRAD the following advantages:

- One less independent parameter;
- Less dependence on the norm of the gradient which can vary in the image
- A natural decrease of the diffusion because the estimated variance of the noise decreases.

3.3 Wavelet Decomposition

Wavelet transform divides the information of an image into approximation and three detail sub signals such as vertical, horizontal and diagonal details. These three sub signals show the details or changes in the image and the approximation sub signal shows the specific tendency of pixel values.

A multilevel 2D Wavelet Decomposition is performed using the Haar filter which returns wavelet decomposition vector C and return its corresponding matrix S. The vector C is organized as follows:

$$C = [A(N) | H(N) | V(N) | D(N) | \dots | A(N-1) | H(N-1) | V(N-1) | D(N-1) | \dots | A(1) | H(1) | V(1) | D(1)] \dots \quad (1)$$

Where A, H, V and D is row vectors such that
 A = approximation coefficients, H = horizontal coefficients,
 V = vertical coefficients and
 D = diagonal coefficients

A basis for each vector space is defined as C_n . The basis function C_n called scaling functions and which is usually denoted by the symbol. A basis for C_n is given by the set of scaled and translated box functions.

3.4 HOP

In this work introduced a new hierarchical oriented prediction (HOP) that combines DPCM with HIP. It provides only resolution scalability but exploits already coded pixels of the same sub-band to improve DE correlation, compared with IWT or HIP.

These modifications concern the previously used threshold that is removed from the definition of the static predictor, and the simplification of the context selection for bias cancelation.

To validate the experiments, three main contributions are discussed: 1) the HOP approach; 2) the sequential context-based error correction; and 3) the entropy coding technique. To improve the shortage of efficiency of the predictors on smooth images, two new extensions, which exploit dynamically constructed predictors employing a least square optimization, also are proposed.

Expectation level of the HOP conspire is acted in two

stages. The first one (H Step) consists of predicting horizontally odd indexed pixels values with the aid of already known pixels: the proposed approach uses not only the even indexed ones but it can also take advantage of any previously predicted ones (which are now causal values).

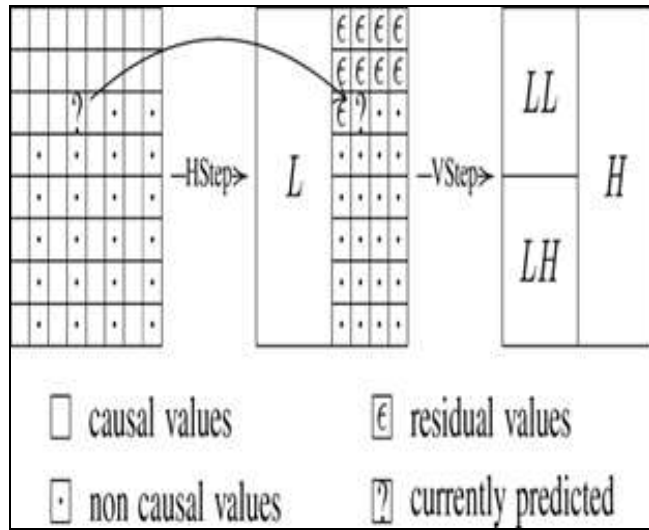


Fig 2: HOP Algorithm Model

Thus, we will obtain a horizontally subsampled image and therefore the residual of the odd predicted pixels. The second step (V Step) is the mathematical transposition of H Step and acts on the lower resolution image.

3.5 HOP-LSE

The HOP’s prediction is not really effective on smooth images. The small prediction support size is not adequate for the DE correlation of diffuse information. Higher order predictors would result in better estimation on such images. To fabricate, the two of them misuse the all-encompassing arrangements of causal pixels contrasted and HOP. For an efficient use of these extended sets, the predictors are dynamically built using least square estimations, giving a better adaptation to the specific characteristics of each image.

3.6 HOP-LSE+

The HOP’s prediction is not really effective on smooth images mainly because the small prediction support size is not adequate for the DE correlation of diffuse information. Because higher order predictors would end in better estimation on such images (using a wider prediction support size).

It reduces the complexity of the algorithm by computing the smallest amount square optimization only. The non-homogeneous areas which represent pixels on the whole data sets allow the division of the computation time. HOP-LSE to create, they both exploit the extended sets of Causal pixels compared with HOP. For an efficient use of these extended sets, the predictors are dynamically built using least square estimations, giving a better adaptation to the specific characteristics of each image.

For HOP-LSE+, the following optimization is always done, whereas for HOP-LSE, if, the non-oriented static predictor of the previous section is used. It reduces the complexity of the algorithm by computing the least square optimization only in the nonhomogeneous areas, which represent about

the pixels on the whole data sets and then allows the division of the computation time, for a non-optimized implementation, by around 3 compared with HOP-LSE.

4. Projected Technique

We propose a predictor based Near-Lossless compression scheme which involves two steps, the first one (H Step) consists of predicting horizontally odd indexed pixels with the aid of already known pixels. The proposed approach uses not only the even indexed ones but it also can cash in of any previously predicted ones (which are now causal values). Thus, we will obtain a horizontally subsampled image and therefore the residual of the odd predicted pixels. The second step (V Step) is the mathematical transposition of H Step and acts on the lower resolution image. Thus we provide a comparative analysis among the three algorithms namely, HOP, HOP-LSE, HOP-LSE+. HOP is usually designed for noisy images containing structured objects with sharp edges (contrasted data), which is that the case for many of native medical images.

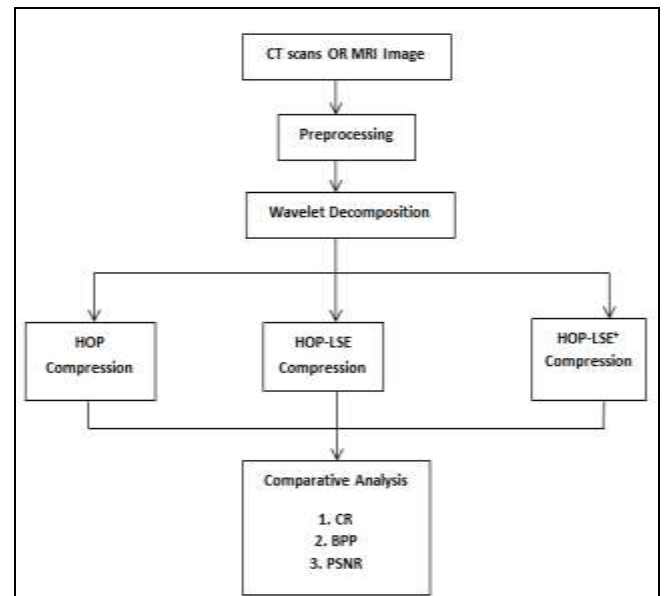


Fig 3: System Architecture Sketch

The approach proposed for HOP may be a combination of the 2 previously mentioned ones. It uses a small set of parameters to quickly estimate the data distribution and to have a rapid coding efficiency, and a wider set of parameters for a slower but better fit to the true distribution, which allows a more powerful compression.

This is done with the aid of two distinct coders used in a two-stage coding as shown in figure. A reduced-parameter entropy coder (stage-0 coder SOC) allows us to quickly approximate the data distribution and to compress the first coefficients where as another coder (stage-1 coder SIC) is learning finer distribution statistics. When the SIC coder is estimated to have sufficiently learned the statistics, it is used instead of SOC for the next coefficients compression.

SIC is continuing to update the data distribution. When a coefficient value is unknown by SIC, an escape symbol is output, and SOC is employed to compress this value. Comparative analysis of our proposal is validated using compression ratio, Bits per pixel and PSNR quality metrics.

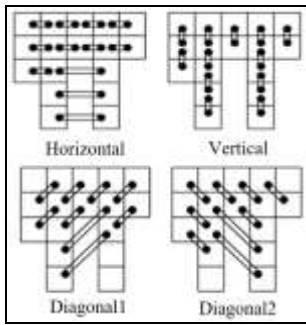


Fig 4: Decomposition Model

5. Results & Discussion

Determine the efficiency of compression using Compression Ratio and Bits per pixel and Peak Signal to Noise Ratio.

5.1 Compression Ratio (CR)

The compression ratio is employed to live the power of knowledge compression by comparing the dimensions of the image being compressed to the dimensions of the first image. It is defined as, $CR = \text{Uncompressed Image} / \text{Compressed Image}$.

5.2 Bits Per Pixel (BPP)

Color depth or bit depth, is a computer graphics term describing the number of bits used to represent the color of a single pixel in a bitmapped image or video frame buffer. This concept is also known as bits per pixel (BPP), particularly when specified along with the number of bits used. Higher color depth gives a broader range of distinct colors.

5.3 Peak Signal to Noise Ratio (PSNR)

The Mean Square Error (MSE) and the Peak Signal to Noise Ratio (PSNR) are the two blunder measurements used to analyze picture pressure quality. The MSE speaks to the aggregate squared mistake between the packed and the first picture, whereas PSNR represents a measure of the peak error.

	CR	BPP	PSNR
HOP	0.3322	24.0822	24.4551
HOP LSE	3.2125	0.3113	47.0934
HOP LSE*	16.8430	2.4750	52.2154

Fig 1: Performance Evaluation

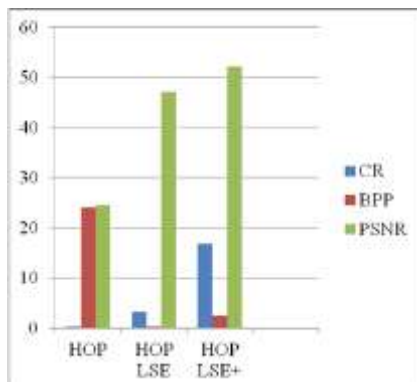


Fig 5: Evaluation Graph

The PSNR block computes the height signal-to-noise, in decibels, between two images. This ratio is usually used as a top-quality measurement between the first and a compressed image. The better-quality image or reconstructed image produced by PSNR

6. Conclusions

A new HOP approach, and two variants using least square optimization (HOP-LSE and HOP-LSE+) have been presented in the context of resolution scalable lossless and NLS biomedical image compression. A new sequential context-based bias cancelation method was proposed and analyzed to enhance the prediction efficiency. The least square optimization has allowed us to spice up the prediction on smooth images, where HOP wasn't really efficient. But HOP algorithm is well suited for NLS compression and provides the high resolution scalable lossless images by HOP LSE+ when compared HOP predictors. Those consequences validated using CR, PSNR and BPP quality metrics.

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